(FILE 'HOME' ENTERED AT 18:19:12 ON 22 DEC 2003)

FILE 'MEDLINE, CANCERLIT, EMBASE, BIOSIS, BIOTECHDS, CAPLUS' ENTERED AT 18:19:27 ON 22 DEC 2003 L140 S ELECTROPORATION CHAMBER L21401525 S ELECTROP? L3161246 S FLOW RATE 1401525 S L2 OR L1 L4L5 2124 S L4 AND L3 L6 1117448 S COMPUTER OR COMPUTATION OR ALGORITHM L7 47 S L6 AND L5 L8 34 DUP REM L7 (13 DUPLICATES REMOVED)

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L8 ANSWER 21 OF 34 MEDLINE on STN DUPLICATE 6

AN 96229040 MEDLINE

DN 96229040 PubMed ID: 8779421

- TI Design of a high-precision fraction collector for capillary electrophoresis.
- AU Muller O; Foret F; Karger B L
- CS Barnett Institute, Northeastern University, Boston, Massachusetts 02115, USA.
- NC GM15847 (NIGMS)
- SO ANALYTICAL CHEMISTRY, (1995 Sep 1) 67 (17) 2974-80. Journal code: 0370536. ISSN: 0003-2700.
- CY United States
- DT Journal; Article; (JOURNAL ARTICLE)
- LA English
- FS Priority Journals
- EM 199609
- ED Entered STN: 19960924 Last Updated on STN: 19960924 Entered Medline: 19960918
- ABA high-precision fraction collector for capillary electrophoresis has been developed. The device utilizes detection close to the end of the capillary and a sheath liquid at the exit of the capillary, allowing continuous collection (i.e., uninterrupted applied electrical field) of multiple species. The role of the sheath liquid flow rate and position of detection in the column on the collection precision was assessed. Fiber-optic detection at approximately 1 cm before the exit end of the capillary was found effective for precise timing of the collection. Up to 60 fractions of microliter or smaller volumes could be automatically collected into capillaries used as collection vials. The collection capillaries were placed on a cylinder, and a computer-controlled stepping motor aligned the appropriate capillary with the column exit. The effectiveness of the fraction collector was demonstrated in the collection of all 11 fragments of the HaeIII restriction digest of phi X-174 plasmid DNA. Polymerase chain reaction amplification of the 271 and 281 bp fragments revealed an inversion of the size-dependent migration order.

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L8
     ANSWER 5 OF 34 CAPLUS COPYRIGHT 2003 ACS on STN
AN
     2001:713653 CAPLUS
DN
     135:254073
TI
     New apparatus and method for electrophysiological testing of
     biological membranes.
IN
     Trumbull, Jonathan D.; Bertrand, Daniel C.; Briggs, Clark A.; Mckenna,
     David G.; Maslana, Eugene S.; Blanchard, David P.; Pan, Jeffrey Y.; Bojan,
     Peter M.; Nemcek, Thomas A.
PA
     Abbott Laboratories, USA
     PCT Int. Appl., 59 pp.
SO
     CODEN: PIXXD2
DT
     Patent
LA
     English
FAN.CNT 1
     PATENT NO.
                    KIND DATE
                                          APPLICATION NO. DATE
                     _ _ _ _
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     WO 2001071312 A2 20010927
WO 2001071312 A3 20020613
PΤ
                                           WO 2001-US9110
                                                            20010321
         W: AU, CA, JP, MX, NO
         RW: AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL,
             PT, SE, TR
     EP 1266219
                      A2
                          20021218
                                          EP 2001-922545 20010321
        R: AT, BE, CH, DE, DK, ES, FR, GB, GR, IT, LI, LU, NL, SE, MC, PT,
             IE, FI, CY, TR
                    T2
     JP 2003528308
                                           JP 2001-569250
                            20030924
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     NO 2002004551
                      Α
                            20020923
                                          NO 2002-4551
                                                            20020923
PRAI US 2000-532686
                      Α
                            20000322
     US 2001-790871
                    W
                      Α
                            20010223
     WO 2001-US9110
                            20010321
AB
     The invention concerns a method and app. for running a plurality of tests
     concurrently to obtain data relating to the electrophysiol.
     properties of receptors and channels in biol. membranes of test subjects,
     such as, for example, Xenopus oocytes. The invention further provides
     software for controlling, acquiring, and recording data relating to
     electrophysiol. properties of receptors and channels in biol.
    membranes of test subjects, such as, for example, oocytes. This invention
     increases the throughput rate for expts. and assays employing receptors
    and ion channels expressed in biol. membranes of test subjects, such as,
    for example, oocytes. In the case of an oocyte, these receptors and
    channels may be natively expressed (endogenous), may be placed into the
    oocyte (exogenous), or may be expressed from other RNA or DNA previously
    placed into the oocyte (exogenous). The invention provides a means for a
    sole researcher to operate a plurality of electrophysiol. test
    stations in the time and space conventionally required by a single
    electrophysiol. test station. The invention automates these
    stations and provides a means for a sole individual to perform large sets
    of expts. that would be phys. and mentally exhausting in the absence of
    this invention. In addn., this invention provides efficient database and
    data anal. software integrated with the data acquisition software, thereby
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increasing the user's data-handling productivity to keep pace with the augmented data generation capacity. Diagrams describing the app. are

given.

Refine Search

Search Results -

Terms	Documents	
L4 same L3	20	

Database:

US Pre-Grant Publication Full-Text Database
US Patents Full-Text Database
US OCR Full-Text Database
EPO Abstracts Database
JPO Abstracts Database
Derwent World Patents Index
IBM Technical Disclosure Bulletins

Search:



Refine Search







Search History

DATE: Monday, December 22, 2003 Printable Copy Create Case

Set Name side by side		Hit Count	Set Name result set
DB=PC	GPB,USPT,USOC,EPAB,JPAB,DWPI; PLUR=YES; OP=A	DJ	
<u>L5</u>	L4 same 13	20	<u>L5</u>
<u>L4</u>	electropo\$	38267	<u>L4</u>
<u>L3</u>	L2 with 11	6444	<u>L3</u>
<u>L2</u>	flow rate or electroporat\$ or variable flux or pulsed energy	422076	<u>L2</u>
<u>L1</u>	computer or computat\$ or algorithm	1373955	<u>L1</u>

END OF SEARCH HISTORY

Generate Collection Print

L9: Entry 44 of 101

File: USPT

Jun 20, 2000

DOCUMENT-IDENTIFIER: US 6078490 A

TITLE: Method of treating materials with pulsed electrical fields

Detailed Description Text (10):

The apparatus employed for carrying out the method of treating material with pulsed electrical fields of the invention includes the Model PA-1000 Electroporation System of Cyto Pulse Sciences, Inc., Columbia, Md., shown in FIG. 1. The Model PA-1000 Electroporation System is designed to accomplish a wide range of electroporation tasks, many of which are not possible with existing equipment. Some of the new tasks that can be carried out by the Model PA-1000 Electroporation System include: changing pulse width from one pulse to the next; changing pulse amplitude from one pulse to the next; changing pulse interval from one pulse to the next; producing a high fidelity pulsed electric field, effectively independent of load; providing a pulse amplitude monitor which gives a very accurate replica of high voltage pulses; providing a pulse current monitor which gives a very accurate replica of pulse current; providing a computer-generated agile pulse sequence; and providing automatic data logging and recall of each pulse sequence used. As a result, the Model PA-1000 Electroporation System provides a sequence of very finely controlled, high fidelity, <u>pulsed</u> electric fields to electroporate a wide variety of substances including plant and mammalian cells.

Generate Collection Print

L9: Entry 48 of 101

File: USPT

Mar 21, 2000

DOCUMENT-IDENTIFIER: US 6041252 A TITLE: Drug delivery system and method

Detailed Description Text (173):

The application of the subthreshold electroporation pulses will desirably be computer driven and allow variation of the appropriate signal strength and duration, and also the number and order of active electrodes which will participate in each pulse. Furthermore, as suggested by Chang in U.S. Pat. No. 5,304,486, the fields (both AC and pulsed RF) may be generated by synthesizing the required electrical wave with a digital computer and amplifying the waveform using a power amplifier. It is anticipated that emphasis may be placed on those electrodes which will effectively concentrate or orient an electrical field in those areas which are deemed to require increased distribution of the facilitory ions due to increased density or decreased blood supply. The exact specifications of intensity of voltage, duration of pulses, number and orientation of pulses will be more fully elucidated as subsequent data are accumulated.

Generate Collection Print

L9: Entry 60 of 101

File: USPT

Aug 12, 1997

DOCUMENT-IDENTIFIER: US 5657119 A

TITLE: Spectrometry using an optical parametric oscillator

<u>Detailed Description Text</u> (7):

FIG. 2 is a block diagram of a thermal lens spectrometer 50 based on a direct incidence system of the type described by K. Mori et al., "Determination of Nitrogen Dioxide by Pulsed Thermal Lens Spectrophotometry" Anal. Chem. 55, 1075-1079 (1983) and by S. Kawasaki et al. "Thermal Lens Spectrophotometry Using a Tunable Infrared Laser Generated by a Stimulated Raman Effect", Anal. Chem. 59, 523-525 (1987). In this spectrometer, the OPO output signal wave 40 from the OPO 10 is used as a pump beam, and is focused into a 1 cm sample flow cell 52 (Hellma Cells, Inc.) by way of a mirror 54, a lens 56, and a quartz wedge 58. A beam 60 from an He-Ne laser 62 (Spectra-Physics, Inc. Model 105-1) is directed to the surface of wedge 58 and is reflected coaxially with the OPO pump beam 40 into the cell 52. The beam 60 is used as the probe beam and passes through the cell without focusing, producing a sample output probe beam 64 which is directed through a quartz prism 66 to a mirror 67. The mirror 67 directs the sample output probe beam 64 through a lens 68 which expands it to a 10 mm diameter, through a pinhole aperture 70, through a polarizer 72 and through a bandpass filter 74 to a photomultiplier 76 (Thorn EMI Electron Tubes, Ltd., 9658R). The pinhole may have an aperture of 1.2 mm, with the bandpass filter being centered at the wavelength of the He-Ne probe; i.e., at 632.8 nm, and with the photomultiplier measuring the intensity of the beam center. The intensity spectrum may be supplied by way of line 80 to a personal computer for display on the computer screen in real time. In a test of the equipment, a sample of nitrogen dioxide (supplied by Matheson) was diluted to 0.5% in dry air and delivered to the flow cell 52 by way of line 82. The flow rate of the sample was 40-50 cc/min and the outlet gas line 84 was then bubbled through an NaOH solution (not shown) and discharged.

Generate Collection | Print

L9: Entry 66 of 101

File: USPT

Sep 27, 1994

DOCUMENT-IDENTIFIER: US 5349946 A

TITLE: Microprocessor controlled flow regulated molecular humidifier

Detailed Description Text (5):

A microprocessor 36 is preferably used to control pulsing valve 30. Microprocessor 36 receives the temperature signal from temperature probe 34 indicating the temperature of the gas and the flow signal from the flow meter indicating the rate of flow of the gas. The flow signal is sent from flow meter 32 to microprocessor 36 via a line 38. The temperature signal is sent from temperature probe 34 to microprocessor 36 via a line 40. Pulsing valve 30 is controlled on or off by the microprocessor in response to these received signals representing the temperature out of the humidifier and the flow rate of gas into the humidifier via an algorithm that causes the microprocessor to calculate an amount of water that is needed to deliver a desired humidity level to the patient for a given rate of flow and temperature of the gas delivered to the patient. Because the gas exiting from ventilator 16 is dry, the algorithm is formulated from the fact that 32 mg H.sub.2 0/l of gas at 37.degree. C. delivers 100% relative humidity. Assuming that all of the water entering humidifier 24 is converted to molecular humidity, then the milligrams of water per minute that need to be delivered to the humidifier to achieve the desired humidity level in the gas delivered to the patient are easily calculated depending on the temperature of the gas flowing out of the humidifier and the liters per minute of gas flowing into the humidifier. Pulsing valve 30 allows a known amount of water to pass through pipe 28 to the humidifier with each pulse or opening of the valve. Therefore, a control signal representing the output of the algorithm is sent to pulsing valve 30 from microprocessor 36 via a line 42 to control the rate at which valve 30 is pulsed. Pulsing valve 30 turns on and off in response to these signals to maintain the water flow to the humidifier such that the desired humidity level is maintained. In this way, the relative humidity of the gas delivered to the patient is regulated.